# Mesenchymal stem cells: potential application in intervertebral disc regeneration

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**Abstract:** Chronic low back pain is one of the leading public health problems in developed countries. Degeneration of the intervertebral disc (IVD) is a major pathological process implicated in low back pain, which is characterized by cellular apoptosis and senescence with reduced synthesis of extracellular matrix (ECM). Currently, there is no clinical therapy targeting the reversal of disc degeneration. Recent advances in cellular and molecular biology have provided an exciting approach to disc regeneration that focuses on the delivery of viable cells to the degenerative disc. Adult mesenchymal stem cells (MSCs) are multipotent stem cells with self-renewal capacities and are able to differentiate into diverse specialized cell types, including chondrocyte lineages. The potential of stem cell therapy in disc degeneration is to repopulate the disc with viable cells capable of producing the ECM and restoring damaged tissue. The present literature review summarizes recent advances in basic research and clinical trials of MSCs to provide an outline of the key roles of MSCs therapies in disc repair. The review also discusses the controversies, challenges and therapeutic concepts for the future.

Keywords: Mesenchymal stem cell (MSC); intervertebral disc (IVD); degeneration; back pain; regeneration

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## Introduction

Chronic low back pain is a widespread condition which affects a large portion of the population and is the predominant cause of disability, resulting in huge cost implications, economic outlay and health provisions (1). Causing approximately \$50 billion of estimated expenditure in the USA alone and with 210,000 Australians developing chronic low back pain annually the costs are increasing, with the direct cost of \$1.2 billion in Australia in 2001 (2,3).

Although the exact cause of back pain remains to be defined, degenerative disc disease is considered to be a predominant source of chronic low back pain (4). The intervertebral discs (IVD) act as shock absorbers during compressive loading of the spine. As the disc degenerates, the spinal column motion segment function decreases, with less load-bearing potential. The disc is an immuno-privileged avascular organ with a low cell density and abundant extracellular matrix (ECM). It is well known that a damaged

disc has a very limited capacity for self-repair. At the cellular level, the degeneration process is characterized by cellular dysfunction accompanied by reduced synthesis of ECM (5).

Disc degeneration is currently managed by non-surgical, conservative treatments or surgical interventions aimed at symptomatic relief and muscular stabilization with no clinical therapy targeting the reversal of disc degeneration (6). Recent advances in stem cell biology and tissue engineering provide an exciting potential approach to bio-regeneration focusing on the delivery of cells capable of restoring disc function.

Considering the limited regenerative capacity of the IVD, suitable sources of cells for regenerative therapies are highly sought after. Adult mesenchymal stem cells or stromal cells (MSCs) are multipotent (7), mainly residing in the bone marrow but also found in many other tissues. Bone marrow MSCs (BM-MSCs) and adipose tissue derived MSCs (AT-MSCs) are highly accessible, there are no ethical

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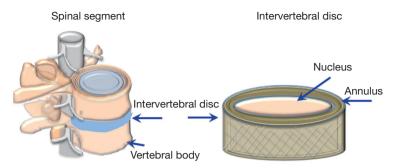


Figure 1 Diagram of the human intervertebral disc.

dilemmas for their use, they have the ability to self-renew, proliferate and differentiate into multiple mature cell types, including chondrocytes (8,9) and have been shown to possess immunomodulatory properties (10). Further, they are able to secrete a variety of soluble mediators and to be recruited chemotactically to injured tissues (11).

MCSs may participate in the repair of degenerative disc tissue in several ways: (I) supply the lost or damaged cells by direct differentiation into disc tissue-specific cells which promote the formation of ECM; (II) indirectly enhance tissue regeneration by the secretion of growth factors; and (III) immuno-modulate the inflammatory response (12). MSC based therapy is emerging as an extremely promising cell therapy for degenerative disc repair. This review aims to provide a better understanding of recent advances in MSC technologies for regenerative therapies in disc degeneration disease, their current challenges and future research directions.

# Intervertebral disc degeneration (IDD)

# Intervertebral disc (IVD)

The IVD is located between the vertebral bodies of the spinal column (*Figure 1*). The properties of the disc allow for spinal mobility and its ability to resist compressive loads, as well as maintaining a uniform stress distribution in the area of the vertebral endplates (EP).

The disc is made up of an inner gelatinous structure, the nucleus pulposus (NP, nucleus) surrounded by a fence-like ring of fibrous laminated collagen, the annulus fibrosus (AF, annulus), sealed superiorly and inferiorly by the cartilaginous EP prior to the vertebral bodies. Each region of the disc has distinct functional structures and complex biological properties (13,14).

The nucleus pulposus is a hydrated gelatinous structure composed of water, ECM, and cellular elements. In

healthy discs, the water content of the nucleus is 80-88% which progressively decreases with age. The NP is derived from the notochord during development. In humans, notochordal cells (Figure 2) disappear in early childhood and differentiate progressively into chondrocyte-like cells (15). The chondrocyte-like cells of the nucleus (Figure 3) are characterised by expression of major ECM components proteoglycans (PG), collagen II, a small amount of elastin fibres (16) and chondrogenic transcription factor SOX9 (17). The main PG within the NP is aggrecan, which contains approximately 30 chains of sulfated glycosaminoglycans (GAGs), contributing to a negative charge that fosters the hyper-hydrated state of the NP (18). NP cells are highly specialized and survive in a hypoxic environment with a high lactic acid concentration as well as relatively high hydrostatic pressure (19).

The AF consists of 15-25 concentric rings of collagen fibrils arranged parallel to each other in a lamellar fashion (Figure 3). Each lamella layer consists of parallel bundles of collagen fibers orientated at about 60° from the vertical axis, with the orientation being reversed in successive lamellae (14,20). The lamellar structure of the AF enables the IVD to withstand the high tensile stresses (circumferential, longitudinal and torsional) the spinal segments are subjected to. The collagen content is at its highest in the outer annulus, comprising up to 70% of its dry weight, with collagen type-I the predominant species, decreasing in a gradient towards the centre of the disc (21). The annulus structure is normally delineated into "outer" and "inner" annulus regions. The inner annulus is less laminar and consists of a more poorly organized ECM that contains type II collagen, PG and water, thereafter a thin fibrous tissue between the inner annulus and the central nucleus has been defined as a transitional zone. Smaller quantities of Type III, V, VI, IX and X collagens are present in the outer AF (22,23).

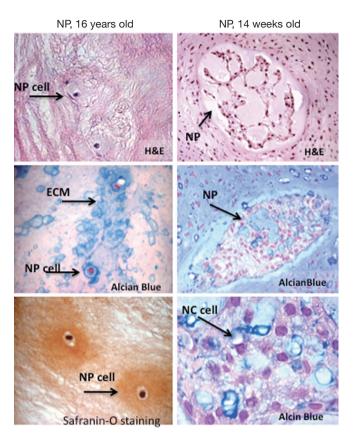


Figure 2 Histological characteristics of healthy human nucleus pulposus. (Left panels) A tissue sample of a healthy human disc from a 16-year-old individual shows sparse chondrocyte-like cells within the nucleus pulposus producing abundant collagen and proteoglycan. Staining with H&E shows morphology (top), Alcian blue (blue staining) identifies proteoglycan (middle) and safranin-O identifies collagen (orange staining, bottom), (magnification 40×). (Right panels) A sample of 14-week-old fetal spine tissue illustrates the NP as highly cellular, containing large vacuolated NC which produce a matrix rich in proteoglycan (magnification 10×, top and middle; 40×, bottom). H&E, haematoxylin & eosin; NC, notochordal cells.

The annulus contains roughly  $9 \times 10^3$  cells/mm<sup>3</sup> of fibroblast-like cells embedded in the outer annulus forming a parallel pattern. More chondrocyte-like cells which are present in the inner annulus (*Figure 2*) (24).

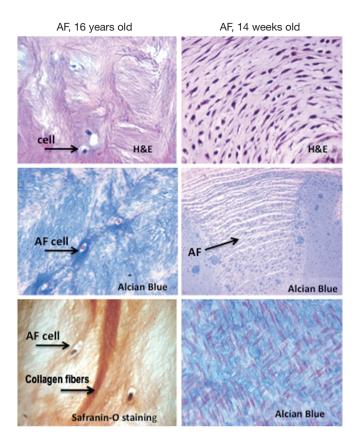
The vertebral EP, composed of 0.6 mm thick avascular hyaline cartilage and fibrocartilage, partially calcified at the vertebral body interface (25), overlies the superior and inferior surface of the vertebral body and is strongly attached to the collagen fibers of the disc annulus. The cells of the EP are chondrocytic. In adulthood, the human EP has the typical structure of an epiphyseal growth plate, acting principally as a growth plate for the vertebral bodies (26). The biochemical components of the EP are similar to that of the disc: water, PG and collagen, but with less proteoglycan and water and higher collagen content than the adjacent regions of the disc. The EP

serves as a semi-permeable membrane to facilitate diffusion of solutes from the vertebrae to the disc, which plays a vital role in disc nutrition by regulating the passive diffusion of nutrients into the avascular disc (25).

# Intervertebral disc degeneration (IDD)

# Back pain and discal degeneration

The degeneration of the delicate structures comprising the IVD is a major cause of back pain. Particularly manifested in the nucleus, changes in disc water content can be visualized using magnetic resonance imaging (MRI), with increasing degeneration visible as increased darkness in the disc region (27). Increasing grade of degeneration has been shown to correlate with back pain (28,29) and the extent of degeneration can be estimated using MRI (27,30-32).



**Figure 3** Histological characteristics of healthy human annulus fibrosus. (Left panels) A sample of a healthy human disc from a 16-year-old individual illustrates the cells in the AF embedded in collagen fibres. Morphology and proteoglycan are visible, (Magnification 40×). (Right panels) A sample of 14-week-old fetal spine tissue showing that the AF has already become well organized into a lamellar pattern (40×, top). Lamellar striations are visible at both low (10×, middle) and high (40×, bottom) magnification when stained with Alcian blue.

A degree of degeneration is attributable to normal aging (28,33,34) and this, coupled with variability in sample sizes, definitions of degeneration and back pain and ethnic genetic diversity are attributed to inconsistent reports of back pain–disc degeneration correlations (35,36).

Certainly the costs related to back pain treatment and lost economic output are reaching the billions globally with the life time prevalence of back pain now approaching 85% (37) and statistics showing it as the main cause of disability worldwide (38).

## The biology of IDD

IDD occurs as a consequence of the normal aging process (34) but can also be instigated by injury trauma (39).

Undoubtedly the main issue in IDD is the deterioration of nucleus pulposus tissue architecture (40,41). Changes are characterised by the loss of gelatinous, hydrated ECM into a more fibrous tissue. PG become fragmented and are lost

from the tissue (14), leading to reduced hydration (42) and a loss of pressure within the nucleus (43). Discal degenerative changes occur progressively as a result of an altered balance between anabolic and catabolic processes in the disc (24,42,44,45). The loss of complex protein and proteoglycan networks that hold water and contribute to the shock absorbing properties in the disc (46), weaken and destabilise the structure contributing to loss of biomechanical function (19,24,47). Ongoing degeneration can lead to herniation, stenosis, segmental instability, and degenerative scoliosis.

Cellular changes: despite obvious tissue deterioration, viable cells isolated from degenerated discs have shown an ability to proliferate and differentiate *in vitro* (48), although with limited regeneration potential (49). Indeed, progenitor cells have been isolated from human degenerated discs (50), potentially derived from specific niche regions located near the cartilaginous end plate (51) and migrating into the disc (52).

Other studies have reported viable cells derived

from degenerated discs with variable morphology but degenerated tissues had increased numbers of cells with the hallmarks of both necrosis and increased cell senescence and apoptosis (40,53,54). Cells were also found to form clusters in degenerated discs, in particular in the NP and inner AF (40,55) and many clustered cells showed increased production of matrix-degrading enzymes such as the matrix metalloproteinases (MMPs) (33,40).

Inflammatory mediators, cytokines & molecular dysregulation: the disc ECM is maintained by a balance of anabolic and catabolic molecular activities (19). In the degenerated disc, the catabolic activity of MMPs, disintegrins, metalloproteinases with thrombospondin motifs (ADAMTSs), and tissue inhibitors of metalloproteinases (TIMPs) is altered, compared to that of normal disc tissue (33,40,56-59), resulting in enhanced breakdown of ECM proteins. These proteins facilitate tissue remodeling in normal disc tissue and are regulated, at least in part, by biomechanical pressure stimuli (33,60,61). Conversely, expression of key ECM components aggrecan and collagen is reduced in degenerated disc tissues (59,62).

Inflammatory mediators, like metalloproteinases, have potential to act as normal growth signals in the normal disc as well as in pathology, but the regulation and expression of these molecules appears to be aberrant in disc degeneration. Increased expression of inflammatory cytokines such as IL-1, IL-6, IL-17 and TNF $\alpha$  have been detected in degenerated disc tissues (63-66) where expression was found in both invading inflammatory cells and resident cells of the NP (63). Degenerated tissues also displayed altered responses to inflammatory cytokines and changed receptor levels (44,62), with only chemokine CXCL8 mRNA expression found to be significantly up-regulated in degenerate compared to non-degenerate samples (63).

The release of chemokines from degenerating discs promotes the infiltration and activation of immune cells, further amplifying the inflammatory cascade and potentially also involving neurogenic factors capable of inducing and enhancing pain effects in the dorsal root ganglion (67). Leukocyte migration into the IVD is accompanied by the appearance of microvasculature tissue and nerve fibres (67) but there is evidence that such invasion is less likely in DDD compared to herniation (40).

Genetic variation in disc degeneration: there is increasing evidence that discal degeneration may be influenced by multiple inherited genetic factors which influence or predispose an individual to the development of this condition (68,69). Several allelic variations in genes coding for ECM proteins have been identified with linkage to degeneration:

asporin, a small leucine-rich repeat proteoglycan (SLRP) family member implicated in several common bone and joint diseases (70,71) has also been identified as a susceptibility gene for discal degeneration (72). Immunohistochemical localization identified asporin in the OAF and less strongly the IAF and showed higher mRNA expression in degenerated discs (73). The ECM protein, cartilage intermediate layer protein (CILP) also showed significant allelic linkage with disc degeneration in a Japanese population (74). CILP is expressed in the disc ECM and levels are elevated in degeneration, increasing as degeneration grade progresses (74,75). Recently an isoform of fibronectin produced by alternative slicing has been linked with degeneration (76) as well as a genetic variant of the sulfotransferase gene (77).

# **Degenerative disc therapies**

# Current therapeutic options

There are no currently available treatments that target disc degeneration itself. Therapeutic interventions are for chronic or acute back pain and are determined by the degree, severity and persistence of pain. A variety of conservative treatment options form initial therapies generally involving rest, pain medication, specialist physiotherapy and/or specific back strengthening which aim to help the spine to heal naturally and in many cases such therapies are successful. However, pain will become chronic (present for more than three months) in approximately 20% of patients and about 5% of chronic back pain sufferers progress to surgical options for further treatment.

Surgical disc treatment mostly involves spinal fusion of two or more disc levels, but technological advancements include more minimally invasive disc replacement therapies that aim to preserve the natural motion of the vertebral segment. Motion preserving devices aimed at supporting the vertebrae by mimicking a normal disc are in limited use and under further development (47,78). The long term success of such devices in preserving existing spinal segments and maintaining full function is not yet known. Biodevices restore some function to the motion segment, however, contrary to expectations the risk of adjacent-level degeneration does not appear to have been reduced (79).

#### Future therapies

The cascade of degeneration being well known and well

documented (24,80), it is attractive to envision the early intervention in discal deterioration by supporting and repairing existing disc tissues biologically, potentially an ideal solution to back pain caused by a loss of disc integrity and function.

# Growth factors

One approach is the application of naturally occurring growth factors capable of stimulating appropriate protein synthesis directly into the disc, restoring tissue integrity and normal pain-free spinal function (81). Candidate proteins for therapeutic discal regeneration have been focused on the bone morphogenetic protein (BMP) family, several of which have shown promise (81-83). BMP13 is one member of this family that appears to play a role in the normal development of the spinal disc in vertebrates (84) and as a result, may have the potential to be a "best in class" molecule for therapeutic application to IDD. BMP13 has shown promise in early large animal studies of annular injury and disc repair (85). The BMP14 molecule is also being trialed as a potential disc regeneration therapeutic (86,87) and investigations into the potential of BMP7 have shown promise (88,89). Clinical grade proteins are proposed to be delivered directly into the disc space. Retention in the disc following injection may depend on many factors, not the least of which is the degree of degeneration and the integrity of the annular ring, data from animal studies is encouraging (85,88). Indeed purified BMP14 protein is currently under phase I/II clinical investigation for the treatment of early stage lumbar disc degeneration in Australia. These studies will provide important validation for the potential of BMP family members as future therapies.

#### Resident stem cells

Several studies have identified progenitor cell populations in the IVD which may provide a source of cells to repopulate a degenerated nucleus, data from animal studies is encouraging the correct stimuli (50,51,90,91). BMP13, following direct injection into the disc in a large animal study, showed evidence of having mobilized cells from the EP region, compared to controls (85) and indeed growth factor therapies rely on endogenous cell populations for their success. Some BMPs can function as chemoattractants (92-94) but involvement of BMP13 in inducing cell migration is still under study. Certainly cell migration into the nucleus pulposus has been reported and may be a valid mechanism for inducing the regeneration of this complex tissue (52,90,95).

# **MSCs** and their regeneration potential

# MSC phenotypes

MSCs are adult stem cells that possess self-renewal ability, multilineage differentiation potential and immunomodulatory properties (7,85,96,97). The term MSCs refers to similar cell populations from multiple tissues that share the basic characteristics of stem cells, but remain heterogeneous cells with variations among individual donors and among different clones from the same donor.

Currently BM-MSCs, followed a close second by AT-MSCs, are major commercial sources of adult MSCs undergoing extensive studies and clinical trials as cell therapies (98-100). MSCs are characterized by the expression of CD73, CD90 and CD105 but lack expression of major lineage markers CD45, CD34, CD14, CD11b, CD79a, CD19 and HLA-DR. They are able to differentiate into multi-lineage specialized cells including osteoblasts, chondrocytes and adipocytes, functions required for a minimal criteria defining these cells (101). Although controversy exists regarding stem cell plasticity (102-104), under appropriate conditions MSCs are not only capable of differentiating into cells of mesenchymal origin (7) but can also trans-differentiate into cells of non-mesodermal lineages such as neuronal cells (104,105) and insulin-producing β-cells (106,107). This has led to the exploration of the therapeutic potential of MSCs for tissue repair in regenerative medicine and as therapeutic tools in immune-mediated diseases (97).

# MSC therapeutic strategies

MSC based therapy aiming to restore damaged tissues relies on not only the ability of MSCs to give rise to specialized lineages, but also on their immunomodulatory and trophic effects. Generally, there are two strategies for the application of MSCs in tissue repair. Firstly, MSCs are used in an undifferentiated state, allowing the cells to undergo differentiation in vivo under the stimulation of local factors. Secondly, MSC differentiation occurs in vitro, prior to transplantation. The disadvantage of the former approach is that unwanted differentiation may occur at the injury site, but prior chondrogenic differentiation can render MSCs phenotypically stable and resistant to trans-differentiation in non-chondrogenic conditions (108). While prior in vitro differentiation ensures MSCs undergo lineage-directed commitment, increasing specificity of the administered cells, the process may affect their immunosuppressive potential (109). In addition, the prolonged cell manipulation

procedure may involve increased risks and costs.

The IVD contains ECM derived from chondrocyte-like cells, but with unique properties, particularly in the central nucleus pulposus (24). Initial attempts at cell implantation using NP cells produced favourable results (110) however, given the limited number of disc cells available and the technical difficulties in their harvest, alternate sources such as MSCs are being pursued. Stem cell therapy involves MSC isolation from an appropriate tissue, in vitro expansion, potentially enhanced by additional growth factors or gene transfer to produce chondrocytic differentiation of the MSCs (111,112). Chondrogenic differentiation of MSCs for seven days produced cells that closely resembled the phenotype of native hyaline cartilage when combined with osteogenic cells in a bilayered oligo [poly (ethylene glycol) fumarate] hydrogel composite (113). Further, the respective chondrogenic and osteogenic phenotypes could be maintained in vitro for 28 days.

# Effective MSC differentiation

Differentiation of MSCs into disc-like chondrocytic cells requires up-regulation of lineage-specific genes and suppression of genes associated with stem cell plasticity. There is a large body of research focused on the efficient induction of MSCs to differentiate into osteo-chondrocyte lineages. Methods of chondrogenic differentiation can be adopted and modified for differentiation of disc-like cells, with various in vitro differentiation conditions established that favour development of this phenotype along with a specific gene/protein expression profile to monitor the differentiation (114), characterised by up-regulation of SOX9 expression followed by chondrogenic specific matrix gene/ protein expression. A three dimensional (3D) culture system and serum-free medium containing transforming growth factor β (TGF-β) and dexamethasone are fundamental conditions for chondrogenic differentiation, with TGF-β3 the most effective compared to other TGF-βs. Some BMPs can enhance TGF-β3-mediated chondrogenic differentiation, but are not effective when used alone (112,115).

MSCs from different individual donors may show various levels of differentiation, even under identical *in vitro* induction conditions. Epigenetic modification, the process of adding and removing chemical tags such as methyl or acetyl groups on DNA or histones which result in specific gene activation or suppression, is one explanation. Genomic regions that contain a high number of methylated cytosine are usually transcriptionally inactive; the absence of DNA

methylation is a prerequisite for transcriptionally active genes (116). Whilst a limited number of studies have been performed, epigenetic regulation mechanisms have been identified in MSC chondrogenesis (117). DNA methylation of CpG-rich promoters associated with chondrocyte-specific genes were largely kept at low levels in human synovium-derived MSCs during *in vitro* chondrogenic differentiation. Further understanding of epigenetic complexities may provide solutions to donor variability, but at present it represents a known source of inconsistency.

# **MSC** application to IVD repair

# Chondrogenic differentiation of MSCs in vitro

MSCs can be induced to differentiate into chondrocytes or disc-like cells *in vitro* using several strategies: utilising co-culturing techniques, cytokine regulation, gene introduction, and 3D culture.

#### Co-culture

MSCs have been co-cultured with disc cells or tissues in vitro either in micromass culture or indirectly, to investigate the compatibility of MSCs in the IVD. Our own studies have demonstrated that rat BM-MSCs can differentiate into NP-like cells after co-culture with intact IVD tissue in a transwell membrane system (118), where although MSCs were separated from disc tissues by an insert membrane they showed morphological cell-cell/cell-tissue interactions via the pores of the membrane, through cytoplasmic processes (Figure 4). The presence of the disc tissue was sufficient to influence the MSCs differentiation pathway and cells from the disc may have provided soluble signalling molecules that influenced MSCs differentiation. Several other studies have co-cultured MSCs and NP cells under different conditions and reported similar observations (119-122). Direct cell-tocell contact in specific ratios was essential for BM-MSC or AT-MSC (123) in monolayer to differentiate into an NPlike phenotype, with enhanced SOX9, aggrecan, collagen II and VI gene expression (111,124). The AT-MSCs may be more capable of differentiating into NP like cells than BM-MSCs (123). Effective chondrogenic differentiation of either umbilical cord blood derived mesenchymal stem cells (hUCB-MSCs) or olfactory stem cells was also achieved by injecting the MSCs into disc tissue in an in vitro culture system (125). Interestingly, even degenerated NP cells in co-culture with BM-MSCs induced increased production of collagen and PG (126).

The underlying mechanisms of cell interactions in

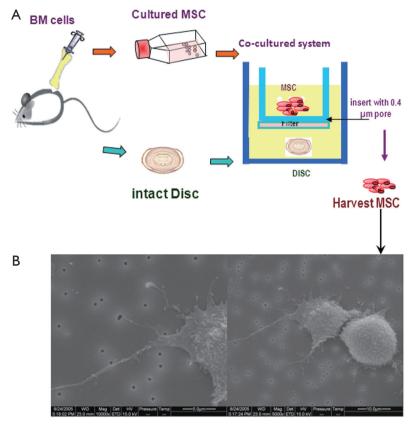


Figure 4 Coculture system and ultrastructural appearance of MSCs following coculture with disc tissue. (A) Schematic diagram of the experimental co-culture process; (B) Ultrastructural appearance of MSCs in co-culture with intact disc tissue, day 14 visualised by scanning electron microscopy. Representative SEM images revealed that most of the co-cultured rMSCs appeared to be spherical or irregular in shape. Some cells have long membrane processes extending from the co-cultured rMSCs through the pores of the transwell-membrane toward the neighbouring disc cells on the underside.

co-culture systems remain unclear, but overall the data suggest that co-culture systems are a powerful tool for the investigation of MSC potential in IVD regeneration. Evidence of bi-directional transfer of membrane components between the cell types, spontaneous cell fusion and gap-junctional communication have been reported, all potentially viable mechanisms (127,128).

# **Growth factors**

A range of growth factors have been employed to induce chondrogenic differentiation of MSCs including TGF- $\beta$ s, insulin-like growth factor-1 (IGF-1), fibroblast growth factor-2 (FGF-2), and BMPs (129). Of these, TGF- $\beta$ 1 has been most extensively investigated for inducing chondrogenesis in stem cells. An early study first reported that MSCs differentiated towards the chondrogenic lineage upon stimulation with TGF- $\beta$ 1 (130) and several studies

have shown TGF-β3 to stimulate MSC to differentiate into chondrocytes (112,129,131) including under hypoxic conditions (131).

Apart from TGF-βs the BMPs, in particular BMP13 (GDF6) and BMP14 (GDF5), have shown MSC chondrogenic differentiation potential. BMP13 stimulation of MSCs in culture induced down-regulation of osteogenic expression markers and promoted higher levels of proteoglycan production (132). Further, undifferentiated MSCs, when treated with BMP13 *in vitro*, induced cellular proliferation and morphological changes resembling chondrocytes at 120 and 168 hours of culture (133). BMP14 possessed a greater ability to induce differentiation of BM-MSCs into NP-like cells than TGF-β under conditions of hypoxia (134). These data suggest that BMP13, unlike BMP2, may not induce the terminal differentiation of stem cells into bone, an attractive characteristic when considering

disc regeneration therapy.

The combination of other growth factors with TGF- $\beta$  has been examined for potential ability to induce MSCs towards a chondrogenic phenotype for use in IVD repair. BMP2 and TGF- $\beta$ 3 induced chondrogenic differentiation of human BM-MSC when cultured in alginate beads (112), and BM-MSC stimulation with BMP7 and TGF- $\beta$ 3 produced superior chondrocytic proteoglycan accumulation, collagen-II, and SOX9 protein expression in alginate and pellet cultures compared to either factor alone (135). Similarly a combination of TGF- $\beta$ 2 and BMP7 was shown to be the most effective combination in inducing AT-MSCs towards chondrogenic differentiation when compared to other factors (136).

# Genetic manipulation

Directing the differentiation of MSCs into specific NP like cells can be achieved by genetic manipulation. SOX9, as an essential transcription factor for the differentiation of the chondrocytic lineage, is required for notochord maintenance and normal vertebral column formation during embryonic development (137). Enhanced chondrogenesis of BM-MSCs was reported both in vitro and in vivo in a mouse model (138) and in human BM-MSCs (139) through over-expression of adenovirus-mediated SOX9. Similarly adenoviral-mediated SOX9 expression induced differentiation into NP-like cells, evident in the expression of chondrogenic genes and proteins (111). More recently BM-MSCs genetically modified with lentiviral-mediated anti-apoptotic GFP-Bcl-2 gene expression showed chondrogenic differentiation in nanofibrous scaffold cultures with TGF-β1 stimulation in hypoxia culture (140). Such studies provide valuable information regarding the appropriate genetic markers and gene regulation required to produce disc cells. However, studies related to disc regeneration are somewhat limited as there are still significant safety concerns regarding the in vivo use of gene therapy (141).

# **Scaffolds**

The application of scaffolds in MSC therapy for disc regeneration will be discussed in section Scaffolds for MSC therapy in disc regeneration.

# MSC therapy for disc repair in vivo

The regenerative potential of MSCs in vivo for disc regeneration has been studied with a variety of animal models by using allogeneic, autologous or xenogenic transplantation (118,142-146). MSCs alone, together with biomaterials or combined with cytokines have been introduced into the disc to attempt both repopulation and repair of damaged cells for the production of new disc matrix.

Survival of transplanted cells is a crucial step to ensure disc repair. Early studies have shown the survival of translocated MSCs in the special microenvironment of a healthy disc for up to six months, as well as their ability to differentiate into NP-like cells (147,148). Multiple *in vivo* studies in a wide array of animal models showed that BM-MSCs can survive and proliferate in the damaged disc post-transplantation. Surviving cells also differentiated towards a disc-like phenotype and produced disc matrix, with partial disc height restoration and hydration when compared to control groups (142,149-156). The use of AT-MSCs with a hyaluronic acid (HA) carrier was also successful, with increased disc matrix protein, restoration of disc hydration and MRI T2 signal intensity eight weeks post transplantation compared to controls (157).

Interestingly, several xenogeneic transplantation studies of human MSCs into murine, porcine or rabbit discs have demonstrated MSC survival without immunosuppressant administration (118,154,158,159). We have demonstrated that transplanted human BM CD34<sup>-</sup> cells survived in rat discs for up six weeks, expressing collagen II and aggrecan after three weeks transplantation (118). The implanted cells had a broad differentiation potential and an ability to develop into disc-like cells, suggesting that CD34<sup>-</sup> BM-MSCs are a potential source of cells for restoring degenerated discs (118). Notably, surviving xenogeneic cells expressed a high level of Fas-L protein, suggested to be an immunosuppressive factor (118).

Successful xenogeneic transplantation also reflects the immune-privileged nature of the disc and the immunosuppressive nature of MSCs (160). The immune privileged nature of the disc is attributed to the anatomically structured blood-tissue barrier of the NP, and also to the constitutive expression of Fas ligand on disc cells (161). *In vivo* studies are encouraging and the data consistent with the potential for the future clinical use for MSCs in IVD regeneration. This data is summarised in *Table 1*.

# Scaffolds for MSC therapy in disc regeneration

Biomaterial scaffolds and hydrogels are three-dimensional matrices. Incorporation of MSCs into a biomaterial scaffold can enhance cell survival after transplantation. The scaffold acts as a carrier protecting MSCs from leaking into other tissues and concomitantly to support the transduction of

Table 1 Overview of recent in vivo animal experimental studies on MSC transplantation for regeneration of the disc

Source of MSC	Animal model & application	Scaffolds	Outcome	Authors and reference
BM-MSC	Rabbit, Autologous	Alelocollagen	MSC survived and differentiated	Sakai et al.
		gel	disc like cells	2003 (149)
	Rabbit (nucleus puncture)	Pure Fibrinous	MSC slowed the rate of disc height	Yang et al.
	Autologous	Gelatin	index	2010 (143)
	Porcine, Autologous	Hydrogel	Regenerate NP and protect the EP	Bendtsen et al.
			function	2011 (144)
	Porcine, Allogenic	HyStem	SPIO labelled MSC present NP by	Barczewska
		hydrogel	MR monitoring	et al. 2013 (156)
	Rabbit, (nucleotomy),	Collagen	MSC survival and matrix production	Yuan et al.
	Allogenic	microspheres		2013 (122)
Expanded	Rabbit (nucleus	Alelocollagen	MSC proliferation and differentiated	Sakai et al.
MSCs	aspiration) Autologous	gel	disc like cells	2006 (155)
Expanded	Canine, (nucleotomy)	No	Suspension disc degeneration	Hiyama et al.
BM MSC	Autologous			2008 (150)
BM-MSC	Mouse, allogenic (annular	No	MSC differentiated chondrocyte and	Yang et al.
from EGFP	puncture)		induce notochondral cells	2009 (146)
transgenic mice				
Human	Mini-pigs (nucleus	Puramatrix	hMSCs survive and express	Henriksson et al.
BM-MSC	puncture) xenogeneic	Hydrogel	chondrocyte markers for 6 months	2009 (154)
	Rat, xenogeneic	No	hMSCs survive in the disc and	Wei et al.
			express chondrocyte markers	2009 (118)
Olfactory	Rat, (nucleus puncture),	No	Observed increased type II collagen	Murrell et al.
neurosphere-	Allogenic			2009 (125)
derived stem cells				
BM-MSC/or	Porcine (nucleotomy)	Fibrin	MSC not found but chondrocyte	Acosta et al.
Chondrocyte	Allogenic		survived and produce CEM	2011 (145)
Human ADSC	Rabbit (nucleus puncture)	Hyaluronate	Elevated extracellular matrix and	Chun et al.
	xenogeneic		little ossification	2012 (159)
ADSC	Rat (nucleus puncture)	PLGA	Partly improve disc height and	Liang et al.
	Allogenic	microspheres	increase ECM of disc after 24 wk	2013 (152)

BM-MSC, bone marrow derived stem cell; ADSC, adipose-derived stem cell; SPIO, superparamagnetic iron oxide nanoparticle.

mechanical loads. They also provide a framework to fertilise proliferation and differentiation of implanted MSCs. To improve the survival of transplanted MSCs, scaffolds need to be non-immunogenic, biodegradable, biocompatible and to withstand the mechanically loaded microenvironment in the IVD (162).

A range of scaffolds have been structured as ideal biomaterials for cell therapy in disc regeneration, including a variety of natural gels and hydrogels based on collagen, HA, GAGs, agarose, gelatine and alginate (163). Hydrogels based on collagen and HA have been the most widely

employed in tissue engineering applications since they are hydrophilic polymers that readily allow for incorporation of biological signals and cells to derive into the native matrix (149,152,155,162). HA is the most abundant water absorption molecule in the natural disc, able to dehydrate and rehydrate under a range of mechanical loading parameters. Such scaffolds also ideally degrade slowly to permit the seeded MSCs to differentiate and produce new matrix (135,162). More recently it was demonstrated that AT-MSCs seeded in chitosan-alginate-gel scaffolds are capable of differentiating into NP-like cells under hypoxic

conditions (164). Similarly, MSC seeded in an injectable hydrogel differentiated along a chondrogenic lineage under physiological loading conditions (165) or when combined with pentosan polysulphate (166,167).

Several hydrogels constructed from natural components of the ECM including fibrin (168), hyaluronan (169), and collagen (170) and natural biopolymers such as chitosan (171) have been investigated as carriers for cell delivery to the disc. Thermoreversible chitosan-glycerophosphate (C/Gp) hydrogels alone are capable of inducing MSC differentiation in cultures (172), and the PEG-LM111 hydrogel in explant cultures showed significantly higher cell retention properties over two weeks, compared to cells in liquid suspension (173).

The therapeutic potential of injectable scaffolds as cell carriers for disc regeneration has been investigated *in vivo* in animal models (149,174,175). Thermoreversible Atelocollagen is composed of 0.3% collagen and, like C/Gp gels, is liquid at room temperature and gelatinizes at body temperature. Transplantation of autologous MSCs encapsulated in Atelocollagen gel into the degenerated disc of a rabbit produced deceleration of the degeneration process (149). Similarly, autologous BM-MSCs embedded in HA-derived biodegradable polymers, Hyaff®-120 and Hyadd®-3 and injected into damaged, nucleotomized porcine discs maintained the normal biconvex structure of the NP and contained viable cells forming a matrix at six weeks, compared to the control group undergoing nucleotomy alone (175).

#### Human clinical trials

MSC transplantation for the treatment of disc degeneration disease in human clinical trials has shown encouraging outcomes. Autologous BM-MSCs have been reported for the first time to treat disc degeneration in two patients with back and leg pain (176), with a collagen sponge containing MSCs transplanted into the degenerated IVD. At two years post-transplantation, pain was reduced and an intradiscal water content increase was observed in both patients. No improvement of disc height was reported.

A pilot phase-1 study in 10 patients (age 35±7 years) with chronic low back pain and lumbar disc degeneration was conducted using autologous BM-MSCs expanded *in vitro* and injected into the NP of degenerated discs, without major surgery (177). After one year of transplantation, pain relief and an improvement in disc hydration (by T2-weighted sagittal images) were observed in nine patients (9/10). The author concluded that MSC therapy may

be a valid alternative treatment for back pain caused by degenerative disc disease. However, disc height was not improved, control groups were not included and evidence of survival of injected cells was also not provided in the trial.

More recently, a multi-centre FDA-approved clinical trial was performed in the United States [2012], including 100 participants with IDD who received a single injection of BM-MSCs encapsulated in a HA carrier, followed for a period of three years.

The outcome of these phase-1 clinical trails is encouraging, suggesting that MSC based therapy is clinically safe and produced relatively effective relief of back pain. However, studies to determine the long term safety and survival of MSCs in the degenerated disc are still needed in order to determine its full potential.

# **Current challenges in MSC therapy**

Although MSCs show great potential in regenerative medicine, issues are emerging regarding quality control and standardization of cells for clinical application. To answer the following questions will be critically important for future safety and efficacy of MSC based therapies.

# Obtaining sufficient cell numbers whilst maintaining MSC characteristics

Adult MSCs exist at extremely low frequency. Although human bone marrow is considered one of richest sources, MSCs only account for 0.001-0.01% of total bone marrow mononuclear cells upon isolation. There is no doubt that therapeutic MSCs must be expanded in vitro to provide sufficient cell numbers (>1×10<sup>6</sup>/kg) without losing stem cell characteristics, which can be judged by examining morphology, cell surface marker phenotypes, multiple differentiation potential, cytogenetic stability and their immunosuppressive property. Recent research suggests that human BM-MSCs in culture maintain their morphology and a stable phenotype until passages 6-8, with some individual donor variation (178). With low propensity for spontaneous transformation, they could be safely expanded in vitro without immortalization or development of chromosomal abnormalities (179,180). However, other studies have suggested a risk of cells accumulating genetic and epigenetic abnormalities beyond passage 4 (181). To date, this issue remains a major challenge for stem cell expansion on a clinical scale.

The use of growth factors or cytokines in addition

to foetal bovine serum (FBS), such as epidermal growth factor (EGF) (182), basic fibroblast growth factor (bFGF), platelet-derived growth factor (PDGF) or ascorbic acid, may boost MSC proliferation and suppress spontaneous differentiation during *in vitro* expansion (183). Importantly, such treatment does not appear to bias future differentiation and immunosuppressive properties of the cells. Our own unpublished data suggests that supplementation of growth factors or cytokines can increase MSC proliferation yielding more than 10-fold higher cell numbers than basic cultures. However, overloading of factors aimed at promoting MSC proliferation may alter cell characteristics.

Most laboratories culture MSCs under normoxia (20% O<sub>2</sub>) conditions. Hypoxic (2-9% O<sub>2</sub>) environments can greatly improve growth kinetics of MSC, multi-lineage differentiation capacity, genetic stability and chemokines receptor expression during *in vitro* expansion (184,185). Optimal formulation of culture medium and conditions for *in vitro* MSC expansion will require further study to ensure optimal yields.

# Standardization of methods for MSC isolation, expansion and characterization

The huge potential of MSC therapy in regenerative medicine has attracted tremendous interest for MSC research. Study methodology, however, lacks coherence in methods of isolation, expansion and characterization making outcomes comparisons difficult, despite the publication of minimal criteria to define human MSCs (101). Variability is largely derived from the following factors.

- (I) Donor variation. Huge variability in proliferative capacity and life span has been noted among donors (179), which is associated with individual genetic and epigenetic variations, age, gender, and health status.
- (II) Tissue variation. MSCs derived from bone marrow, adipose or other tissues are similar, but not identical.
- (III) Isolation methods. Ficoll-Paque gradient centrifugation (1.077 g/mL) is included in most MSC isolation methods to obtain mononuclear cells, followed by further enrichment by plastic adherence for three days. In addition to this basic procedure extra purification steps may be added, such as immune-depletion or positive selection using monoclonal antibodies.
- (IV) Cell culture media. Basic MSC culture medium contains 10% FBS but can be up to 20%. In addition, the source and lot number of FBS provides increased variability in cell growth, reflecting considerable variations in

- composition of growth factors and other trophic factors in the serum.
- (V) Oxygen pressure. MSCs are mostly cultured in ambient normoxia conditions. Currently though, more and more laboratories are realising the advantages of culturing MSCs under hypoxia (2-5% O<sub>2</sub>), conditions which influence cellular aging and composition leading to altered MSC functions.

Donor variation in MSCs is unavoidable but variability can perhaps be minimised by determining standard selection criteria and MSC expansion methodology. Such measures are extremely necessary in order to ensure reproducibility of MSC preparations and a high level of therapeutic efficacy.

# How pure should the MSC population be?

No matter which method is applied to isolate MSCs, they are by nature a heterogeneous cell population containing a small percentage of stem cells and many other differently committed progenitors. These cells present heterogeneity in morphology, phenotype and multipotentiality. It remains unclear whether heterogeneous MSC populations are good enough or whether pure stem cells are required for clinical use. It is conceivable that heterogeneity contributes to their various therapeutic effects (186), However, clonogenic MSC subpopulations have been studied, showing that a CD73+/CD39+ human synovial MSCs subset displayed greater chondro-osteogenic potency (187).

# Low engraftment rate, disadvantage or advantage?

Although the fate of MSCs after clinical infusion is not fully understood, MSCs have a relatively short life in the recipient and engraftment rates are low. To improve therapeutic efficacy, should we focus on increasing engraftment rates or improving MSC quality? In wound repair studies, although MSC differentiation occurred at injury sites, most of the therapeutic effects were attributed to soluble factors released by the administered cells which regulate local cellular responses to cutaneous injury (188). It was also observed in a clinical study that there was no correlation between MSC engraftment and treatment response, with MSCs appearing to mediate their function through a "hit and run" mechanism. Fortunately, the lack of sustained engraftment limits the long-term risks of malignant transformation and ectopic tissue formation during MSC therapy (189).

It remains to be established whether MSCs can differentiate into disc NP cells, with their precise phenotype and chondrocytic markers. Current evidence regarding MSC therapy for IVD repair is from small animal studies which may not resemble human disc degeneration.

#### **Summary**

MSC therapy for disc repair has made significant progress over the last several years with regards to further understanding of stem cell biology and the different applications of MSCs for the treatment of low back pain. MSCs have been reported to be effective *in vitro* for the differentiation of disc like cells. In addition, *in vivo* transplantation of MSCs has been shown to have regenerative potential in several animal models for disc degeneration. Overall, the recent advances in MSC therapies suggest a promising future for such therapies in disc repair.

Notably it has been suggested that injection of chondrocytes into the NP resulted in the formation of hyaline cartilage but not a gelatinous matrix (190), emphasizing that the direction of the MSCs towards NP cell fates is essential for effective disc repair. Moreover, the disc has unique anatomical characteristics and biological properties and much remains unknown about the molecular mechanisms and interactions in the degenerated disc, as well as the mechanisms of action behind the therapeutic effects of MSCs. In this regard, it may be beneficial for more efforts to focus on further investigating the survival of transplanted cells in the damaged disc niche, the molecular regulators and signalling pathways controlling proliferation and cell fates following transplantation, and the appropriate integration of the transplanted cells within their surrounding microenvironment

Although the current clinical literature involves only small sample sizes, phase-1 clinical trails of MSC therapy for low pack pain have provided certain positive outcomes for disc repair. These cases are valuable studies for creating a foundation to direct future experimental and clinical investigations. Importantly, safety remains one of the main concerns, particularly in view of the necessary *in vitro* manipulation of MSCs, such as for cell expansion. Thus, before any clinical application can be recommended, improved knowledge from basic studies and large scale randomized trials with controlled implementation will be necessary to determine the true safety and efficacy of cell therapies in IVD regeneration.

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#### **Footnote**

*Conflicts of Interest*: The authors have no conflicts of interest to declare.

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